



SOLUBILITY AND DISSOLUTION ENHANCEMENT OF KETOTIFEN BY SOLID DISPERSION TECHNIQUE

Fergany A. Mohamed, Dina F. M. Mohamed and Omnia A. E. Mahmoud*

Department of Pharmaceutics, Faculty of Pharmacy, Assiut University, Assiut 71526, Egypt

Ketotifen (KT) solid dispersions and physical mixtures were prepared with the objective of solubility and dissolution improvement using Hydroxypropyl-Beta-Cyclodextrin (HP- β -CD), Pluronic 127 (PF-127), Pluronic 68 (PF-68), Polyethylene glycol 6000 (PEG 6000), and Polyethylene glycol 4000 (PEG 4000). The saturation solubility and in-vitro dissolution studies showed remarkable improvement in solubility and drug dissolution of these new solid dispersions and physical mixtures over pure ketotifen. The XRD, DSC, IR and SEM studies indicated the transformation of crystalline ketotifen (in pure drug) to amorphous ketotifen (in solid dispersions). This study concluded that the improved solubility as well as drug dissolution of these new ketotifen solid dispersions may be attributed to improved wettability and reduction in drug crystallinity, which can be modulated by appropriate level of hydrophilic carriers.

INTRODUCTION

Nearly 40% of the new chemical entities currently being discovered are poorly water-soluble drugs¹. Most formulation strategies for such drugs are targeted at enhancing their dissolution rate and/or solubility by achieving their fine dispersion at absorption level². Bioavailability of a drug depends on its solubility and/or dissolution rate, and dissolution may be the rate-determining step for the onset of therapeutic activity^{3&4}. Therefore, poorly aqueous soluble drugs are usually characterized by low bioavailability due to their lower absorption⁵. Enhancement of bioavailability can be attained by various approaches to improve drug solubility as well as drug dissolution.

Numerous techniques have been used to increase the solubility of poor water soluble drugs which include micronization in which the enhancement of drug absorption is done via reducing its particle size^{6&7}, formation of inclusion complexes of drugs with α -, β -, γ -cyclodextrins by coprecipitating and spray-drying^{8&9}, formation of the amorphous form of the drug which is a highly energetic form of the drug and usually has a lower melting point and

a higher dissolution rate than the stable crystal form¹⁰, formation of drug solid dispersions¹¹⁻¹³ as supersaturated systems by using diverse types of carriers, ranging widely from water-soluble to amphiphilic to lipid-soluble ones¹⁴⁻¹⁸. Solid dispersion is a group of solid products consisting, generally, of a hydrophobic drug and hydrophilic matrix¹⁹⁻²¹. Fast and immediate drug dissolution from solid dispersions has been observed due to increased wettability and dispersibility of drug particles, existence of the drug in amorphous form with improved solubility, and absence of aggregation of drug particles using various hydrophilic carriers²²⁻²⁵.

Ketotifen is a widely used antiallergy drug with a variety of biological effects, including the inhibition of the release of myotonic mediators, leukotrienes in particular; the inhibition of slow reacting substances- induced bronchoconstriction *in-vivo*, calcium antagonistic properties, and the prevention or reversal of decreased beta-adrenoceptor sensitivity²⁶. Ketotifen belongs to the second-generation H1-antihistamine drugs²⁷.

Ketotifen has chemical structure shown in figure 1. The molecular weight of its free form is 309.43 and the Log P is 2.2²⁸.

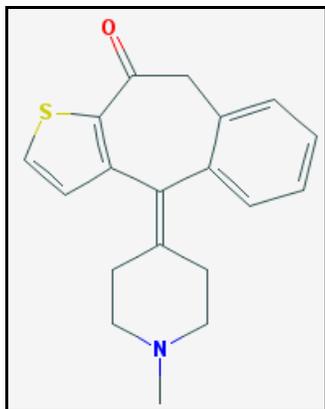


Fig. 1: The chemical structure of ketotifen.

Ketotifen is widely used as tablets, capsules, syrups, nasal drops and eye-drops (as fumarate salt). Oral ketotifen formulation is usually administered twice a day, and the dosing usually lasts for several years with daily dose of 2 mg, and the bioavailability is about 50% in humans²⁹. Therefore, there is a significant need for the development of a more convenient dosage form for children, ketotifen suppository.

The objectives of this investigation are: (i) preparation of ketotifen solid dispersions and physical mixtures, (ii) characterization of newly prepared ketotifen solid dispersions and physical mixtures by X-ray diffraction (XRD), Differential scanning calorimetry (DSC), Fourier transform infrared spectroscopy (FTIR), and Scanning electron microscopy (SEM), and (iii) estimation of drug solubility and evaluation of drug dissolution of prepared ketotifen solid dispersions and physical mixtures to compare these data with pure drug data.

EXPERIMENTAL

Materials

- Ketotifen was supplied from Pharco Co., Egypt.
- Hydroxypropyl- β -cyclodextrin was supplied from Sigma Chemi CO; Germany.
- Pluronic F-127(PF-127) and pluronic F-68 (PF-68) were supplied from Sigma-Aldrich Chemie, Germany.
- Polyethylene glycol (PEG 6000, PEG 4000) were supplied from Sigma Chem. CO., USA.
- All chemicals were of pharmaceutical grade and were used as received.

Methods

Preparation of ketotifen solid dispersions by solvent evaporation technique

Solid dispersions of ketotifen (KT) with different polymers: Hydroxypropyl- β -cyclodextrin, Pluronic F-127 (PF-127), pluronic F-68 (PF-68), Polyethylene glycols (PEG 6000, PEG 4000) at various weight ratios (1:1, 1:3, 1:5, 1:7) were prepared by the solvent evaporation method as follows. Weighed quantity of KT was dissolved in a minimum amount of absolute ethanol; the appropriate amount of each polymer was added. The resulting mixture was stirred until evaporation on magnetic stirrer and then the co-precipitates were then scrapped and stored in a desiccator over anhydrous CaCl_2 , to constant weight. The evaporated product was ground in a mortar and passed through a sieve and stored in a desiccator until further evaluation. A specified sample of the prepared solid dispersion was assayed for the drug content.

Determination of percent drug content

Weight amount of solid dispersions, each sample equivalent to 5 mg of ketotifen were separately taken and added to 10 ml of ethanol in stoppered conical flasks. The sealed flasks were agitated on a rotary shaker for 1 hr. The solution was diluted with ethanol and was assayed by a UV-VIS spectrophotometer for drug content at 301 nm using the following expression: Percent drug content = (actual drug content in solid dispersions / theoretical drug content in solid dispersions) x 100.

Preparation of ketotifen physical mixtures

Ketotifen (KT) and solid carriers were sieved through 180 μm sieve, and then the physical mixtures in the ratios (1:1, 1:3, 1:5 and 1:7) were prepared by simple, gentle mixing using spatula and paper method. A specified sample of each prepared physical mixture was assayed for the drug content.

Determination of solubility

Saturated solubility of pure ketotifen (KT) was determined and then compared with these data of ketotifen solid dispersions and physical mixtures of respective ratios. The known excess samples (ketotifen solid dispersions, physical mixtures and pure ketotifen), 10 mg equivalent weight of ketotifen was added to 10

ml distilled water in a glass beaker covered with foil and these samples were rotated at 100 rpm in a water bath (37±0.5°C) for 24 hrs. The samples were then filtered through 0.45 µm membrane filter, suitably diluted, and analyzed by UV-VIS spectrophotometer at 301 nm wavelength. All experiments were carried out in triplicate.

Dissolution studies

Dissolution studies of pure ketotifen (KT), ketotifen solid dispersions and physical mixtures of different ratios were studied using U.S.P. XXIV (U.S.P., 2000) dissolution apparatus II (paddle type). Weighed amounts equivalent to 10 mg of KT were dispersed over 500 ml of phosphate buffer pH 7.4 at 37±0.5°C and stirred at 100 rpm for 2 hrs. At fixed time intervals, samples (2 ml) were withdrawn and equal amount of fresh dissolution medium was added. Withdrawn samples were filtered through 0.45 µm membrane filters, and spectrophotometrically assayed for drug content at 301 nm wavelengths using a UV-VIS spectrophotometer. All experiments were carried out in triplicate. The cumulative amount of the drug dissolved during the n^{th} sample (Q_n) was estimated by the following equation:

$$Q_n = C_n \cdot V + V_s \cdot \sum_{i=1}^{n-1} C_i$$

Where C_n is the measured concentration in the n^{th} sample, V is the volume of dissolution medium and V_s is the volume of sample^{26&27}.

Fourier transform infrared spectroscopy (FTIR)

FTIR spectra of drug alone, the selected physical mixtures and solid dispersions were done at the scanning range of 400-4000 cm^{-1} . Potassium bromide (KBr) disk method was used. The samples were ground, mixed thoroughly with KBr and compressed at a pressure of 6 ton/ cm^2 using IR compression machine.

Differential scanning calorimetry (DSC) analysis

The samples were analyzed by DSC-50 differential scanning calorimeter (Shimadzu, Seisakusho Ltd, Kyoto, Japan). Samples (3-5) mg were accurately weighed into solid aluminum pans and heated at a scanning rate of

10°C /min from 0-300°C in the presence of nitrogen at a flow rate of 20 ml/min.

Transition temperature (°C) and heats of fusion of melting endotherms on the thermograms were calculated using the DSC-T50 program, which directly integrates the melting endothermic peaks giving the heat of fusion (ΔH , Joule/g).

Powder-X-ray diffraction (p-XRD) studies

Powder X-ray diffraction patterns were recorded on an X-diffractometer Phillips PW 1050 (Bragg-Brentano), the radiation used was generated by a copper $K\alpha$ filter, with a wavelength of 1.5418 Å at 40 mA and 35 kV. Samples were scanned over a range of 2θ values from 4° to 60° at a scanning rate of 0.06°/min.

Scanning electron microscopy (SEM)

The SEM analysis was carried out using a JSM- 6400 (Jeol, Japan) by coating the samples with a thin layer of gold using ion sputtering at 15 kV. Digital images of the samples were obtained.

RESULTS AND DISCUSSION

Determination of solubility

The Amount solubilized of KT in water at 37°C from its solid dispersions (SD.) and physical mixtures (P.MIX.) using different carriers at different drug: carrier ratios (1:7, 1:5, 1:3, 1:1) are displayed in tables 1,2.

It is clear that HP-β-CD > PF-127 > PF-68 > PEG 6000 > PEG 4000 in solubilizing effect on KT. Also it was noted that as the amount of polymer increased, the amount of drug solubilized increased.

The maximum amount solubilized was in solid dispersion containing 7 parts of HP-β-CD. The high affinity to HP-β-CD might be due to the hydrophilicity of HP-β-CD, which gave good adjustment of KT to the cyclodextrin cavity. The higher solubilizing effect of PF-127 over PF-68 could be due to more lipophilicity of PF-127 than PF-68 resulting in more interaction with lipophilic part of KT³⁰. In the case of PEG 6000 the hydrophilic effect increased with the increase in the polymer chain than PEG 4000, supporting the humectation of the drug leading to enhancement in aqueous solubility.

Table 1: Solubility of ketotifen (KT) from its solid dispersions (SDs.) with different carriers in water at 37°C.

Carrier	Amount solubilized of KT (mg/ml)			
	1:7	1:5	1:3	1:1
PF-127	0.225 ± 0.087	0.195 ± 0.044	0.183 ± 0.019	0.154 ± 0.023
PF-68	0.189 ± 0.013	0.165 ± 0.032	0.142 ± 0.076	0.124 ± 0.091
PEG 6000	0.180 ± 0.042	0.151 ± 0.079	0.118 ± 0.083	0.112 ± 0.0112
PEG 4000	0.157 ± 0.063	0.133 ± 0.071	0.103 ± 0.094	0.094 ± 0.056
HP-β-CD	0.408 ± 0.083	0.342 ± 0.076	0.301 ± 0.023	0.157 ± 0.099

Solubility of KT in water at 37°C was **0.0411** mg/ml.

Table 2: Solubility of ketotifen (KT) from its physical mixtures (P.MIXs.) with different carriers in water at 37°C.

Carrier	Amount solubilized of KT (mg/ml)			
	1:7	1:5	1:3	1:1
PF-127	0.195 ± 0.083	0.159 ± 0.097	0.139 ± 0.015	0.124 ± 0.067
PF-68	0.145 ± 0.066	0.115 ± 0.045	0.103 ± 0.074	0.094 ± 0.09
PEG 6000	0.136 ± 0.0563	0.1 ± 0.029	0.088 ± 0.02	0.068 ± 0.076
PEG 4000	0.118 ± 0.0354	0.091 ± 0.078	0.077 ± 0.0299	0.047 ± 0.0432
HP-β-CD	0.337 ± 0.059	0.284 ± 0.084	0.248 ± 0.043	0.136 ± 0.085

Solubility of KT in water at 37°C was **0.0411** mg/ml.

Dissolution studies

The dissolution of KT in phosphate buffer (PH 7.4) at 37°C and from its solid dispersions (SD.) and physical mixtures (P.MIX.) using different carriers at drug: Carrier ratios (1:7), (1:5), (1:3) and (1:1) are displayed in tables 3-10 and figures 2-9. The results obtained show that:

The improvement of dissolution rates of KT by different carriers was ranked as: HP-β-CD > PF-127 > PF-68 > PEG 6000 > PEG 4000.

The percent of drug dissolved from solid dispersions (SD.) was higher than the percent of drug dissolved from physical mixtures (P.MIX.) which in turn was higher than that dissolved from the untreated drug.

Dissolution rate of KT increased by increasing the ratio of the carrier used. This is might be due to conversion of the drug from crystalline form into an amorphous one. Also might be due to the particle size reduction of the drug. Moreover, polymers encircling the drug leading to decrease the aggregation of drug particles allowing faster dissolution.

Fourier transform infrared spectroscopy (FT-IR)

In the IR spectrum illustrated in figure 10. KT shows its characteristic peaks at 3097.1 cm⁻¹ assigned for thiophene group Stretching, 3000-2840 cm⁻¹ assigned to aromatic stretching, 1650 cm⁻¹ for carbonyl group³¹.

The spectrum of HP-β-CD illustrated an intense broad band at 3500-3300 cm⁻¹ corresponding to the free -OH stretching vibration³².

The spectra of pluronic copolymers (Figs. 11-12) showed broad band of -OH stretching vibration from 3330 to 3710 cm⁻¹ for PF-127 and 3355-3610 cm⁻¹ for PF-68. C-H stretching of OCH groups from 2900 to 3095 cm⁻¹ and C-H stretching from 1058 to 1144 cm⁻¹³³.

The IR spectra of PEG 4000 and PEG 6000 (Figs. 13-14) showed a characteristic band at 3000 cm⁻¹ corresponding to -OCH₃ stretching³⁴.

The spectra of the physical mixtures (P.MIX.) at the ratio of 1:7 of KT with different polymers were superposition of pure components spectra, indicating the absence of interaction between KT and any polymer used³⁵.

Table 3: Shows *in-vitro* dissolution of pure KT and its solid dispersions with different carriers at ratio 1:7 (drug : carrier) in phosphate buffer at 37°C.

Time (min.)	% Dissolved of Ketotifen (KT)					
	Drug alone	HP- β -CD	PF-127	PF-68	PEG 6000	PEG 4000
5	22.03 \pm 0.465	99.97 \pm 0.231	85.17 \pm 0.924	81.799 \pm 0.555	73.05 \pm 0.144	70.98 \pm 0.228
10	24.14 \pm 2.061	100 \pm 0.456	94.94 \pm 1.89	90.55 \pm 1.077	76.71 \pm 0.153	75.4 \pm 0.678
15	27.61 \pm 2.412	100 \pm 1.096	100 \pm 0.633	99.89 \pm 2.613	84.69 \pm 0.333	80.85 \pm 2.642
30	33.42 \pm 2.069	100 \pm 0.672	100 \pm 1.021	100 \pm 0.285	91.49 \pm 1.98	86.699 \pm 1.782
60	38.33 \pm 1.957	100 \pm 0.343	100 \pm 0.103	100 \pm 0.178	94.04 \pm 1.53	90.32 \pm 1.851
120	40.25 \pm 3.888	100 \pm 0.906	100 \pm 1.001	100 \pm 1.808	99.86 \pm 0.036	93.98 \pm 0.912

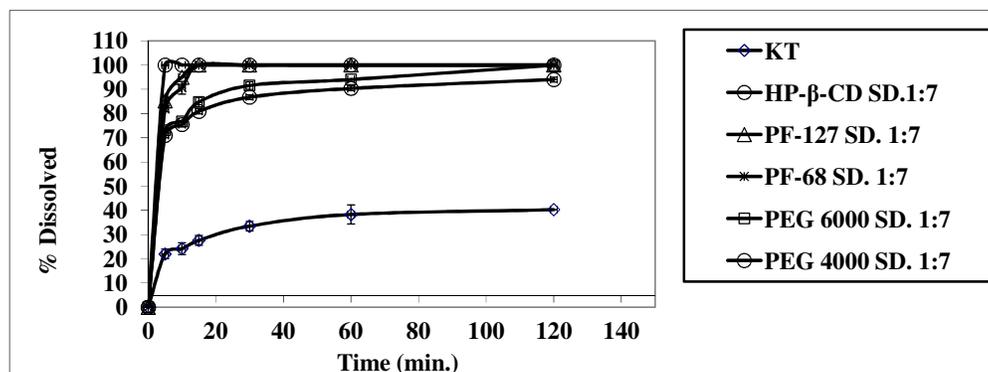


Fig. 2: Shows *in-vitro* dissolution profiles of pure KT and its solid dispersions with different carriers at ratio 1:7 (drug: carrier) in phosphate buffer at 37°C.

Table 4: Shows *in-vitro* dissolution of pure KT and its solid dispersions with different carriers at ratio 1:5 (drug: carrier) in phosphate buffer at 37°C.

Time (min.)	% Dissolved of Ketotifen (KT)					
	Drug alone	HP- β -CD	PF-127	PF-68	PEG 6000	PEG 4000
5	22.03 \pm 0.465	98.49 \pm 1.122	81.9 \pm 0.993	78.14 \pm 0.224	70.92 \pm 1.239	64.03 \pm 0.345
10	24.14 \pm 2.061	99.3 \pm 0.786	92.4 \pm 1.541	80.68 \pm 0.768	74.81 \pm 2.604	69.17 \pm 0.752
15	27.61 \pm 2.412	100 \pm 0.539	96.1 \pm 1.023	83.75 \pm 2.675	77.63 \pm 1.783	73.31 \pm 1.006
30	33.42 \pm 2.069	100 \pm 0.34	99.33 \pm 2.043	89.73 \pm 0.923	81.59 \pm 0.945	79.12 \pm 0.982
60	38.33 \pm 1.957	100 \pm 0.681	100 \pm 0.971	92.33 \pm 1.033	86.42 \pm 1.845	83.11 \pm 0.347
120	40.25 \pm 3.888	100 \pm 0.0237	100 \pm 0.084	96.71 \pm 1.785	88.89 \pm 1.312	85.68 \pm 0.189

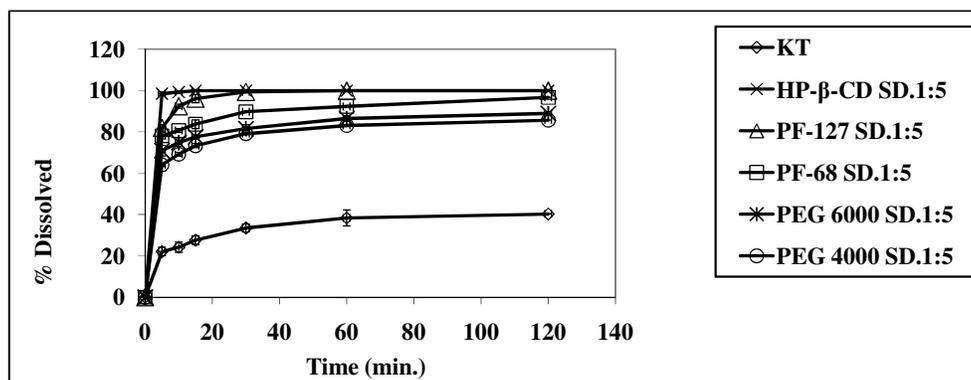


Fig. 3: Shows *in-vitro* dissolution profiles of pure KT and its solid dispersions with different carriers at ratio 1:5 (drug: carrier) in phosphate buffer at 37°C.

Table 5: Shows *in-vitro* dissolution of pure KT and its solid dispersions with different carriers at ratio 1:3 (drug: carrier) in phosphate buffer at 37°C.

Time (min.)	% Dissolved of Ketotifen (KT)					
	Drug alone	HP-β-CD	PF-127	PF-68	PEG 6000	PEG 4000
5	22.03 ± 0.465	91.09 ± 1.137	80.13 ± 0.184	73.44 ± 0.275	60.49 ± 0.986	57.14 ± 1.098
10	24.14 ± 2.061	95.77 ± 0.952	84.11 ± 0.241	75.02 ± 0.179	61.30 ± 1.2785	59.33 ± 2.003
15	27.61 ± 2.412	98.54 ± 0.291	86.47 ± 0.168	76.19 ± 0.154	65.17 ± 1.504	60.11 ± 1.613
30	33.42 ± 2.069	100 ± 0.725	89.07 ± 0.173	80.37 ± 0.184	69.33 ± 0.6733	64.12 ± 0.556
60	38.33 ± 1.957	100 ± 0.82	90.88 ± 0.278	84.74 ± 0.122	71.41 ± 0.954	68.05 ± 1.093
120	40.25 ± 3.888	100 ± 0.63	93.98 ± 0.497	85.98 ± 0.144	75.03 ± 0.2938	69.99 ± 0.394

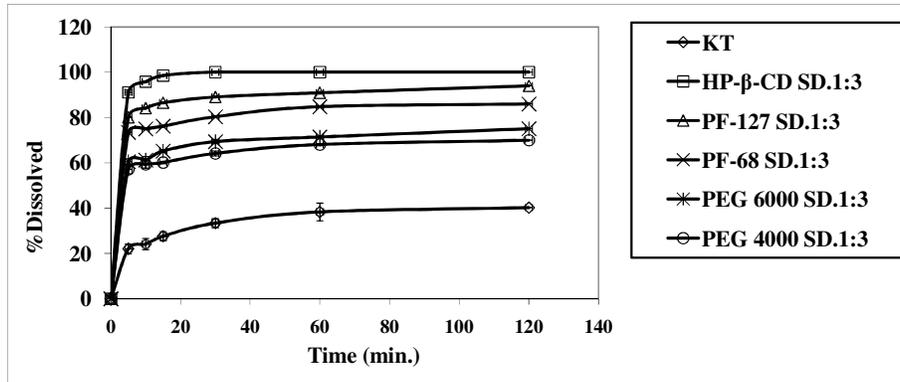


Fig. 4: Shows *in-vitro* dissolution profiles of pure KT and its solid dispersions with different carriers at ratio 1:3 (drug: carrier) in phosphate buffer at 37°C.

Table 6: Shows *in-vitro* dissolution of pure KT and its solid dispersions with different carriers at ratio 1:1 (drug: carrier) in phosphate buffer at 37°C.

Time (min.)	% Dissolved of Ketotifen (KT)					
	Drug alone	HP-β-CD	PF-127	PF-68	PEG 6000	PEG 4000
5	22.03 ± 0.465	89.02 ± 0.3544	67.42 ± 1.467	59.79 ± 0.761	58.90 ± 2.178	53.81 ± 0.782
10	24.14 ± 2.061	93.06 ± 0.2499	69.22 ± 2.964	62.04 ± 1.453	59.99 ± 1.239	54.41 ± 0.459
15	27.61 ± 2.412	95.96 ± 0.7237	72.63 ± 1.004	65.87 ± 1.249	60.28 ± 0.942	55.90 ± 1.379
30	33.42 ± 2.069	97.88 ± 0.3608	76.20 ± 0.9504	68.18 ± 0.974	63.78 ± 0.641	61.24 ± 1.746
60	38.33 ± 1.957	100 ± 0.569	77.97 ± 0.348	71.55 ± 1.735	66.90 ± 1.677	62.93 ± 0.894
120	40.25 ± 3.888	100 ± 0.72	81.10 ± 1.515	73.91 ± 1.345	69.07 ± 1.291	65.17 ± 0.537

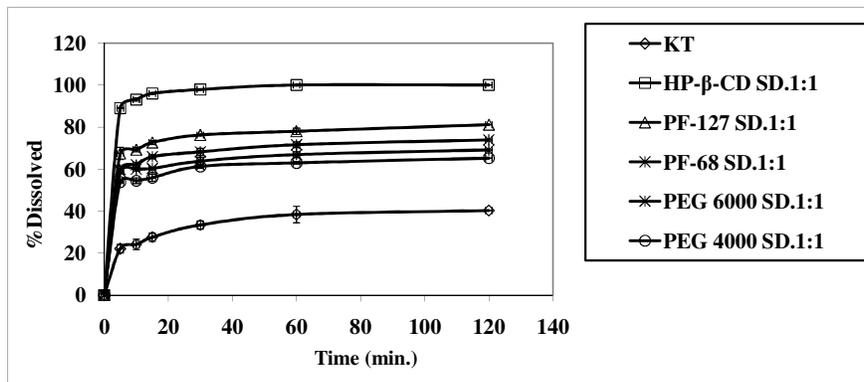


Fig. 5: Shows *in-vitro* dissolution profiles of pure KT and its solid dispersions with different carriers at ratio 1:1 (drug: carrier) in phosphate buffer at 37°C.

Table 7: Shows *in-vitro* dissolution of pure KT and its physical mixtures with different carriers at ratio 1:7 (drug: carrier) in phosphate buffer at 37°C.

Time (min.)	% Dissolved of Ketotifen (KT)					
	Drug alone	HP-β-CD	PF-127	PF-68	PEG 6000	PEG 4000
5	22.03 ± 0.465	82.2 ± 0.87	72.4 ± 0.576	67.3 ± 0.889	63.57 ± 0.355	58.55 ± 1.267
10	24.14 ± 2.061	94.5 ± 0.9111	84.88 ± 1.912	76.11 ± 0.495	70.97 ± 1.908	65.5 ± 0.435
15	27.61 ± 2.412	99.19 ± 2.652	94.32 ± 2.345	85.63 ± 0.777	75.82 ± 1.008	68.59 ± 0.966
30	33.42 ± 2.069	100 ± 0.712	100 ± 1.014	91.96 ± 0.233	82.55 ± 2.542	74.26 ± 1.89
60	38.33 ± 1.957	100 ± 0.903	100 ± 0.71	98.96 ± 0.288	87.4 ± 1.099	79.5 ± 0.964
120	40.25 ± 3.888	100 ± 1.89	100 ± 0.443	99.87 ± 0.972	93.96 ± 0.367	82.95 ± 0.563

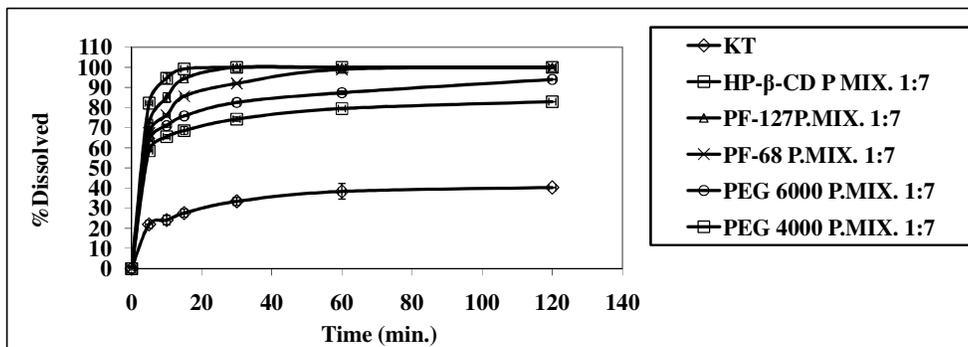


Fig. 6: Shows *in-vitro* dissolution profiles of pure KT and its physical mixtures with different carriers at ratio 1:7 (drug: carrier) in phosphate buffer at 37°C.

Table 8: Shows *in-vitro* dissolution of pure KT and its physical mixtures with different carriers at ratio 1:5 (drug: carrier) in phosphate buffer at 37°C.

Time (min.)	% Dissolved of Ketotifen (KT)					
	Drug alone	HP-β-CD	PF-127	PF-68	PEG 6000	PEG 4000
5	22.03 ± 0.465	77.03 ± 1.2784	69.98 ± 2.011	66.11 ± 0.783	60.08 ± 1.187	56.91 ± 1.844
10	24.14 ± 2.061	80.22 ± 0.8153	72.14 ± 0.918	70.03 ± 0.914	61.39 ± 1.834	58.08 ± 1.983
15	27.61 ± 2.412	82.40 ± 0.9144	79.21 ± 0.734	75.19 ± 1.340	65.02 ± 0.723	59.92 ± 2.431
30	33.42 ± 2.069	96.01 ± 0.3987	85.90 ± 1.145	81.06 ± 1.921	74.48 ± 0.980	63.18 ± 1.313
60	38.33 ± 1.957	99.91 ± 0.2143	89.90 ± 1.632	83.97 ± 0.873	83.57 ± 1.058	69.96 ± 1.007
120	40.25 ± 3.888	100 ± 0.93	95.01 ± 0.653	89.99 ± 0.659	85.32 ± 2.30	71.98 ± 0.786

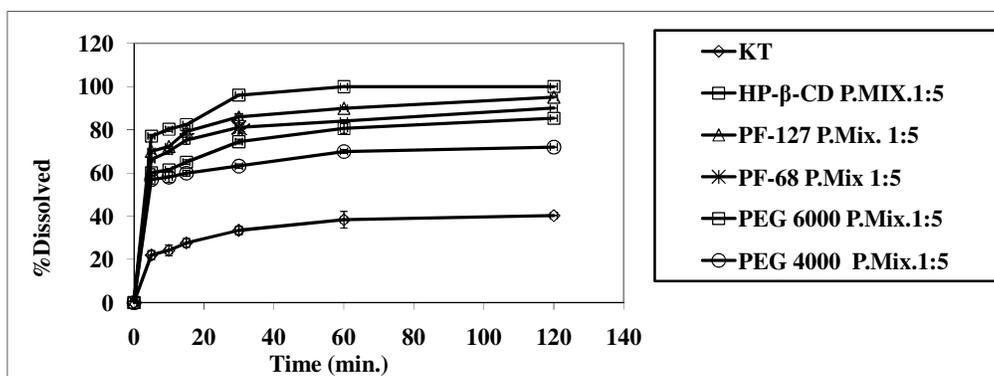


Fig. 7: Shows *in-vitro* dissolution profiles of pure KT and its physical mixtures with different carriers at ratio 1:5 (drug: carrier) in phosphate buffer at 37°C.

Table 9: Shows *in-vitro* dissolution of pure KT and its physical mixtures with different carriers at ratio 1:3 (drug: carrier) in phosphate buffer at 37°C.

Time (min.)	% Dissolved of Ketotifen (KT)					
	Drug alone	HP-β-CD	PF-127	PF-68	PEG 6000	PEG 4000
5	22.03 ± 0.465	73.9 ± 1.041	63.45 ± 0.448	64.23 ± 2.003	57.43 ± 1.824	40.4 ± 0.445
10	24.14 ± 2.061	78.15 ± 1.1454	71.02 ± 1.1276	65.90 ± 0.982	58.97 ± 1.671	41.97 ± 0.676
15	27.61 ± 2.412	79.97 ± 0.843	75.14 ± 0.8452	67.11 ± 0.634	60.15 ± 0.569	43.67 ± 0.926
30	33.42 ± 2.069	90.03 ± 1.9201	83.55 ± 0.9134	74.59 ± 1.409	64.22 ± 1.091	48.79 ± 0.328
60	38.33 ± 1.957	95.13 ± 0.5233	87.62 ± 0.567	77.42 ± 2.281	66.71 ± 0.875	50.78 ± 0.993
120	40.25 ± 3.888	98.44 ± 0.794	91.42 ± 0.9978	79.17 ± 0.869	70.19 ± 0.349	56.09 ± 1.165

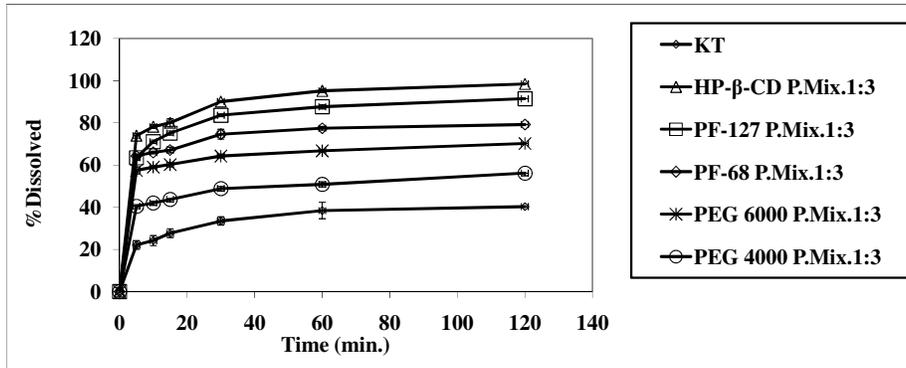


Fig. 8: Shows *in-vitro* dissolution profiles of pure KT and its physical mixtures with different carriers at ratio 1:3 (drug: carrier) in phosphate buffer at 37°C.

Table 10: Shows *in-vitro* dissolution of pure KT and its physical mixtures with different carriers at ratio 1:1 (drug: carrier) in phosphate buffer at 37°C.

Time (min.)	% Dissolved of Ketotifen (KT)					
	Drug alone	HP-β-CD	PF-127	PF-68	PEG 6000	PEG 4000
5	22.03 ± 0.465	70.81 ± 1.0987	61.69 ± 1.813	60.33 ± 2.005	51.24 ± 1.571	38.73 ± 0.820
10	24.14 ± 2.061	76.30 ± 0.6721	63.22 ± 0.843	63.09 ± 1.249	52.5 ± 0.449	40.02 ± 0.649
15	27.61 ± 2.412	80.01 ± 0.7906	66.82 ± 0.239	65.87 ± 0.398	55.94 ± 0.846	41.57 ± 1.762
30	33.42 ± 2.069	83.45 ± 1.1802	71.97 ± 0.911	70.17 ± 1.278	59.22 ± 1.222	47.39 ± 0.673
60	38.33 ± 1.957	89.78 ± 2.117	74.44 ± 1.188	73.26 ± 0.874	62.48 ± 0.983	49.98 ± 1.132
120	40.25 ± 3.888	93.16 ± 0.985	78.89 ± 1.937	77.56 ± 0.568	67.87 ± 0.773	53.18 ± 2.009

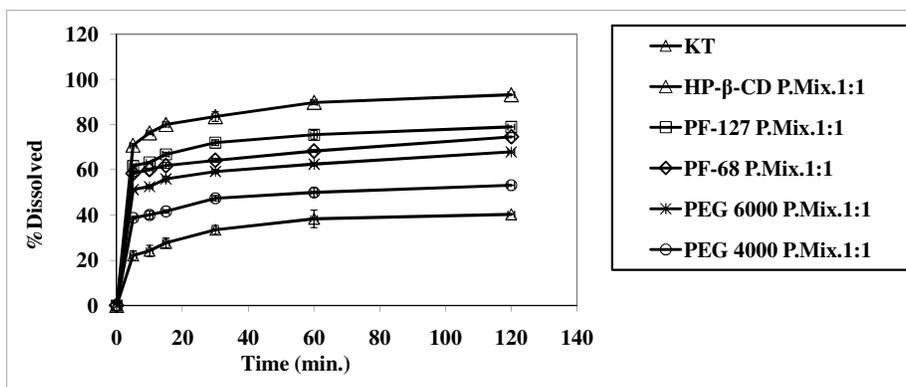


Fig. 9: Shows *in-vitro* dissolution profiles of pure KT and its physical mixtures with different carriers at ratio 1:1 (drug : carrier) in phosphate buffer at 37°C.

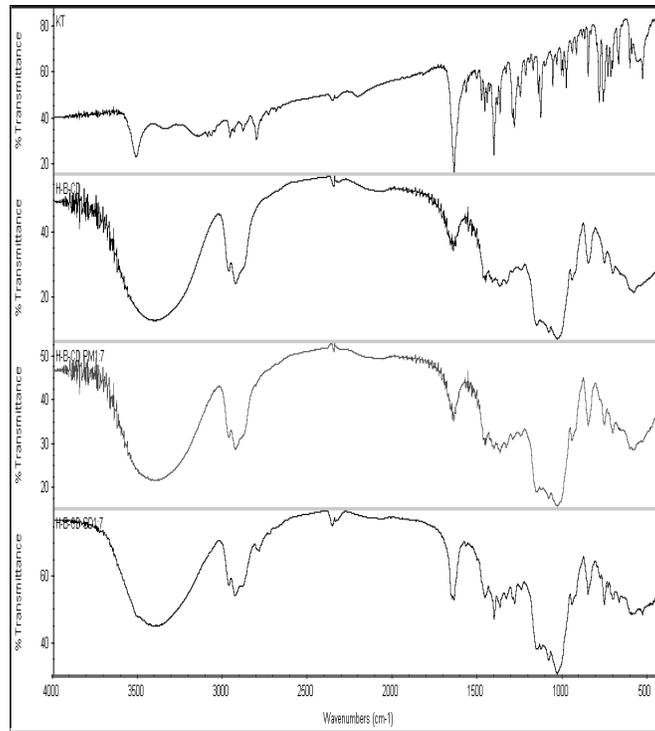


Fig. 10: Comparative study of the FTIR spectra of (a) pure drug KT; (b) HP- β -CD polymer; (c) P.MIX. 1:7; and (d) SD. 1:7.

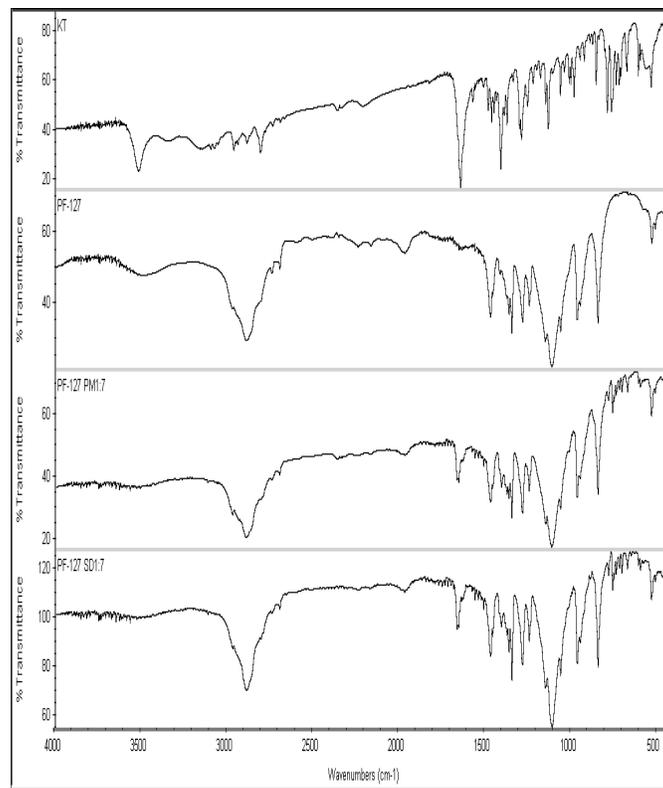


Fig. 11: Comparative study of the FTIR spectra of (a) pure drug KT; (b) PF-127 polymer; (c) P.MIX. 1:7; and (d) SD. 1:7.

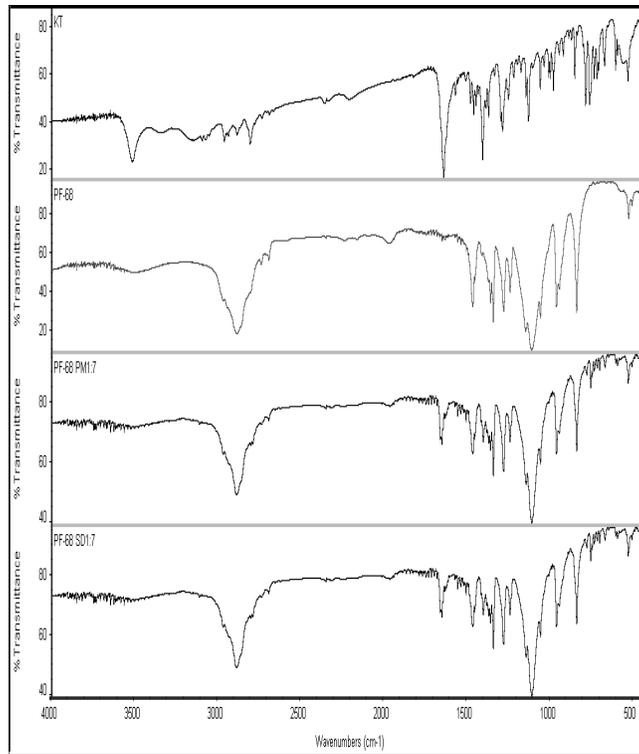


Fig. 12: Comparative study of the FTIR spectra of (a) Pure drug KT; (b) PF-68 polymer; (c) P.MIX. 1:7; and (d) SD. 1:7.

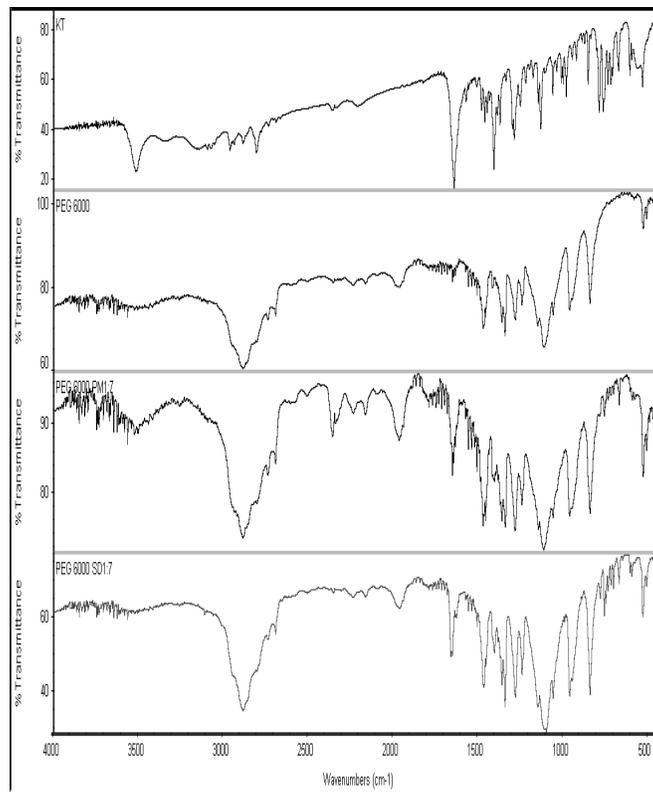


Fig. 13: Comparative study of the FTIR spectra of (a) pure drug KT; (b) PEG 6000 polymer; (c) P.MIX. 1:7; and (d) SD. 1:7.

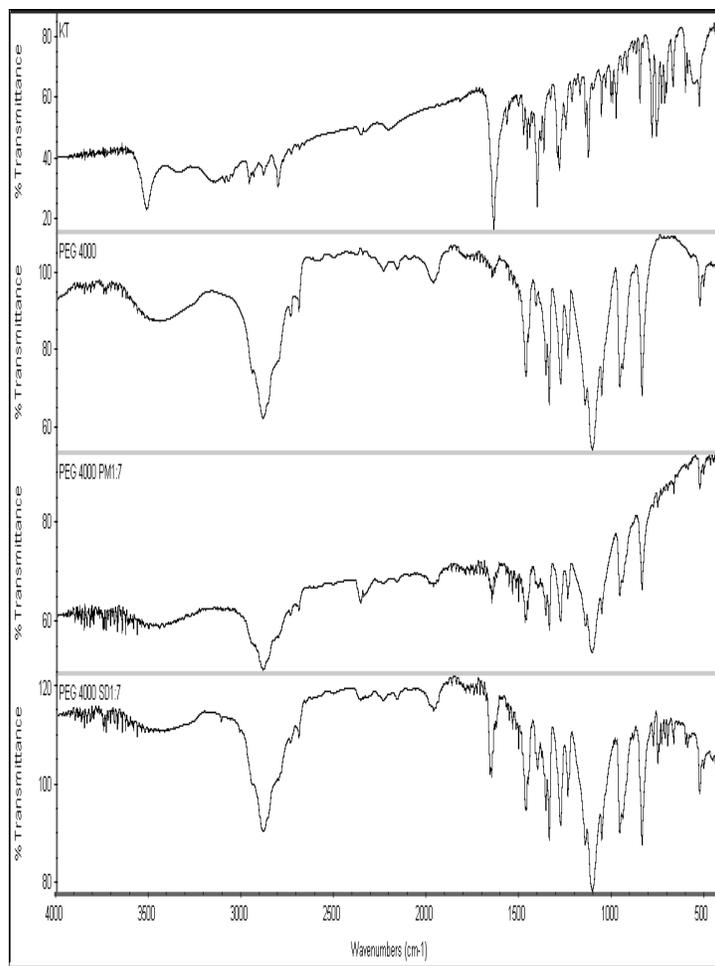


Fig. 14: Comparative study of the FTIR spectra of (a) pure drug KT; (b) PEG 4000 polymer; (c) P.MIX. 1:7; and (d) SD. 1:7.

The IR spectra of KT solid dispersions (SD.) at the ratio of 1:7 showed the band of thiophene strongly stretched, this is might explained by the dissociation of the intermolecular hydrogen bonds associated with crystalline drug molecules and there was a decrease in intensity of drug's aromatic stretching this is might be due to the restriction of KT within the polymer cavity.

Differential scanning calorimetry (DSC) analysis

The DSC thermograms of drug (KT), different polymers (HP- β -CD, PF-127, PF-68, PEG 6000 and PEG 4000) as individual components, as well as drug: Carrier (1:7) solid dispersions and the corresponding physical mixtures are shown in figures 15-19. Table 11

shows the endothermic peaks and ΔH of KT, HP- β -CD, PF-127, PF-68, PEG 6000 and PEG 4000, their corresponding solid dispersions and physical mixtures at ratio (1:7).

KT thermogram showed endothermic peak at 157°C ³¹. While the melting point of the pure polymers are 51.87, 53.6, 60.35 and 64.45°C for PF-68, PF-127, PEG 4000 and PEG 6000, respectively^{33&34}. In the case of HP- β -CD owing to its amorphous nature, a broad endothermic peak was observed at about 100°C corresponding to water loss³⁶.

The DSC curves of the solid dispersions and physical mixtures showed one peak corresponding to the melting point of the polymers. The disappearance of the endothermic peak of KT melting in solid dispersions confirmed the presence of KT in an

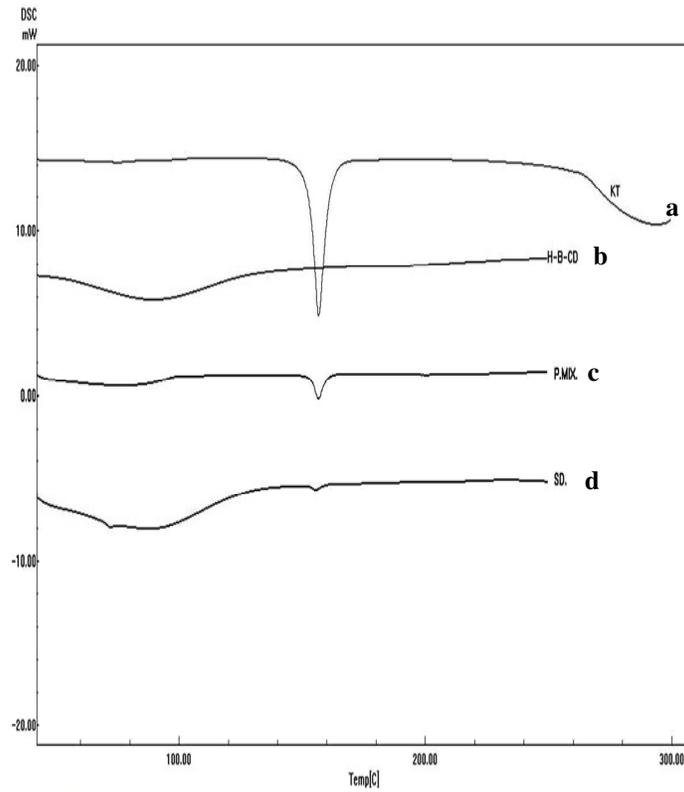


Fig. 15: Shows DSC thermograms of (a) pure drug KT, (b) HP-β-CD polymer, (c) physical mixture of KT with HP-β-CD 1:7, (d) solid dispersion of KT with HP-β-CD 1:7.

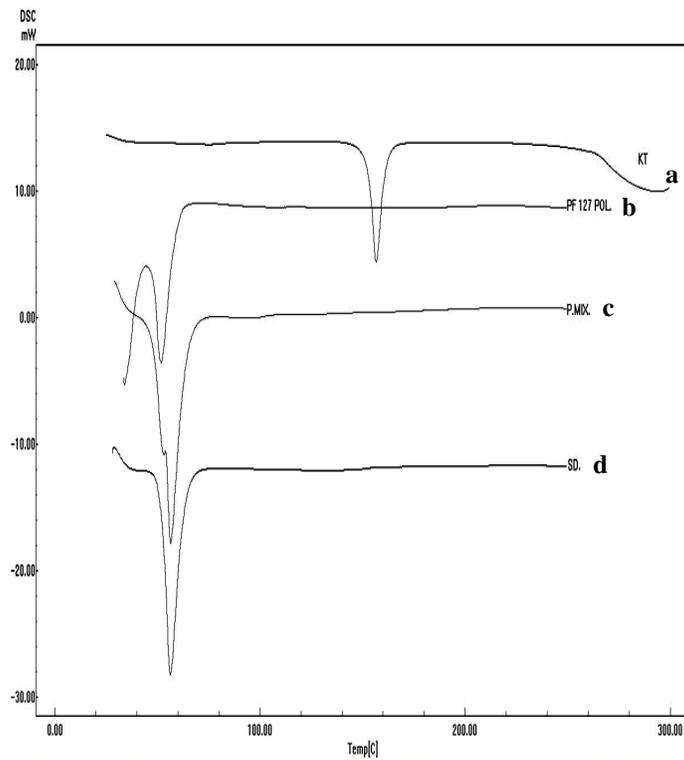


Fig. 16: Shows DSC thermograms of (a) pure drug KT, (b) PF-127 polymer, (c) physical mixture of KT with PF-127 1:7, (d) solid dispersion of KT with PF-127 1:7.

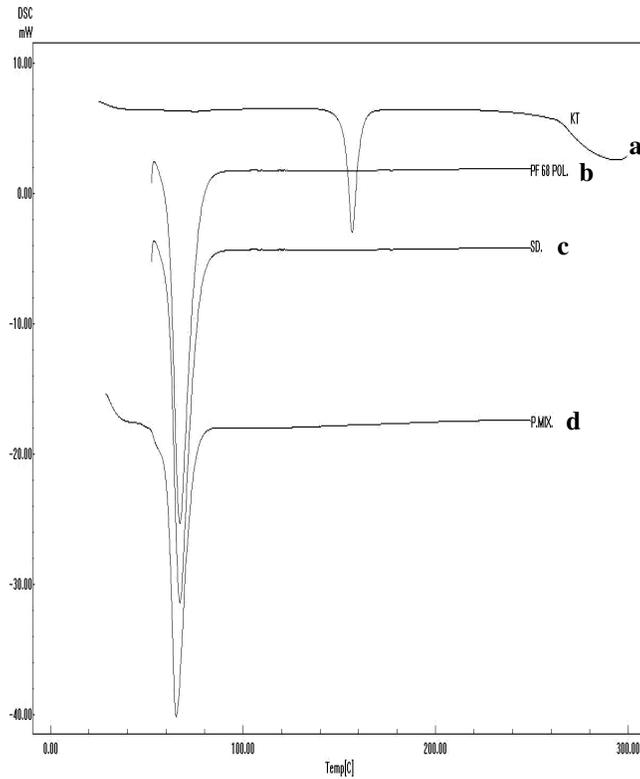


Fig. 17: Shows DSC thermograms of (a) pure drug KT, (b) PF-68 polymer, (c) solid dispersion of KT with PF-68 1:7, (d) physical mixture of KT with PF-68 1:7.

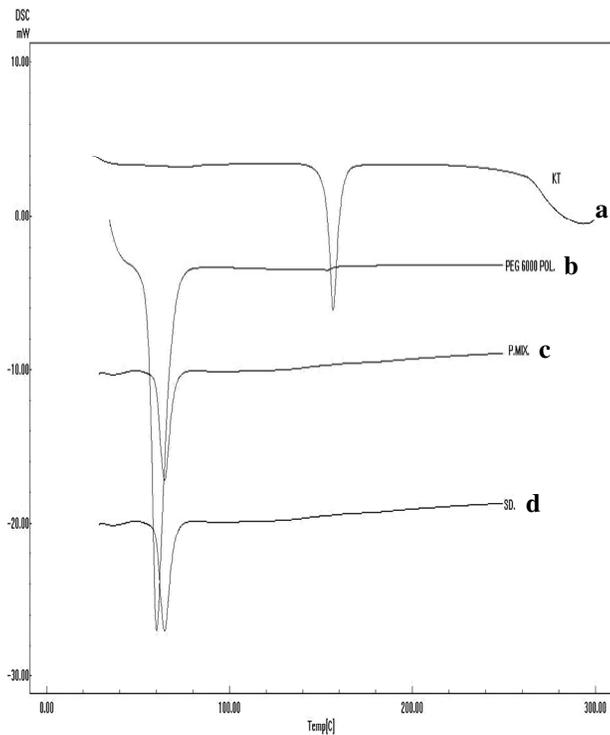


Fig. 18: Shows DSC thermograms of (a) pure drug KT, (b) PEG 6000 polymer, (c) physical mixture of KT with PEG 6000 1:7, (d) solid dispersion of KT with PEG 6000 1:7.

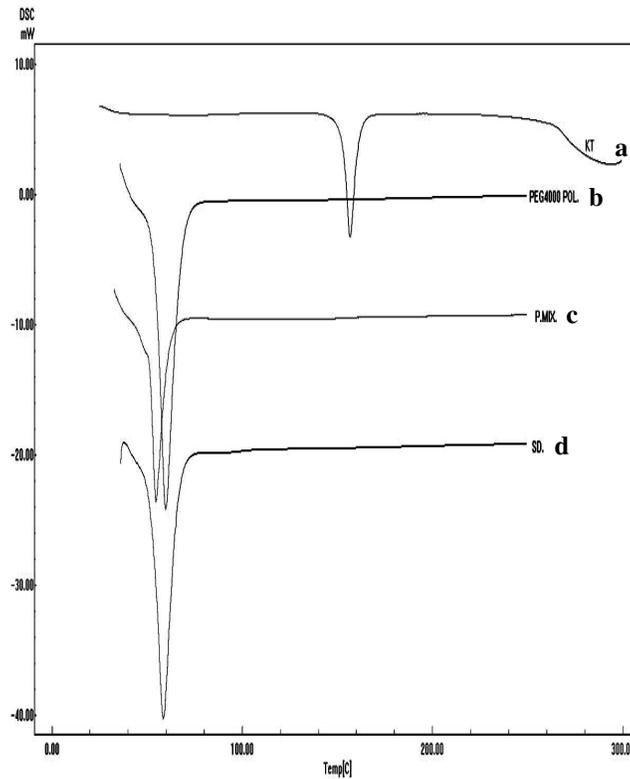


Fig. 19: Shows DSC thermograms of (a) pure drug KT, (b) PEG 4000 polymer, (c) physical mixture of KT with PEG 4000 1:7, (d) solid dispersion of KT with PEG 4000 1:7.

Table 11: the endothermic peaks and ΔH of KT, HP- β -CD, PF-127, PF-68, PEG 6000, and PEG 4000, their corresponding solid dispersions and physical mixtures at ratio 1:7.

System	Onset point (°C)	Endothermic peak (°C)	ΔH (J/ g)
KT	149.97	157	-83.45
HP-β-CD	80.38	89.86	-125.8
KT/ HP-β-CD (1:7) SD.	78.38	86.51	-90.56
KT/ HP-β-CD (1:7) P.Mix.	79.52	83.45	-101.49
PF-127	47.27	53.6	-126.0
KT/ PF-127 (1:7) SD.	46.09	52.49	-71.74
KT/ PF-127 (1:7) P.Mix.	46.51	52.99	-89.13
PF-68	45.91	51.87	-104.52
KT/ PF-68 (1:7) SD.	46.77	51.6	-80.73
KT/ PF-68 (1:7) P.Mix.	44.97	50.18	-69.37
PEG 6000	58.45	64.45	-184.9
KT/ PEG 6000 (1:7) SD.	57.68	63.93	-99.14
KT/ PEG 6000 (1:7) P.Mix.	57.98	64.05	-87.98
PEG 4000	52.75	60.35	-147.93
KT/ PEG 4000 (1:7) SD.	51.89	59.96	-132.11
KT/ PEG 4000 (1:7) P.Mix.	52.51	60.13	-100.19

amorphous form. However, the disappearance of the endothermic peak of KT melting in physical mixtures could be due to its solubility in the melted polymer. Moreover, the similarity between results obtained for solid dispersions and physical mixtures confirmed the absence of interaction between KT and all the polymers used.

Powder-X-ray diffraction (p-XRD) studies

X-ray diffractograms of KT, HP- β -CD, KT/HP- β -CD 1:7 SD and corresponding KT/HP- β -CD 1:7 P.Mix. are shown in (Fig. 20). Diffractograms confirmed the crystalline nature of KT³¹ while HP- β -CD was presented as an amorphous structure^{32,35&36}. The diffractogram of physical mixture (P.Mix.1:7) could be considered as a superposition of the pure components with some variation in shape and intensities of the peaks. However, the observed lower intensity of the peaks may be due to particle size reduction during mixing and dilution of the pure crystalline components. On the other hand the diffractogram of solid dispersion (SD. 1:7) showed a disappearance of crystalline pattern of KT.

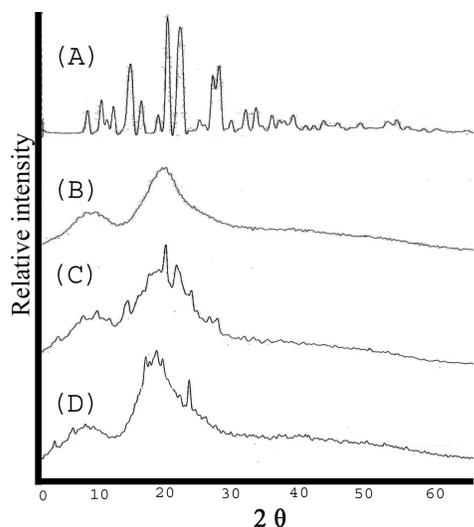
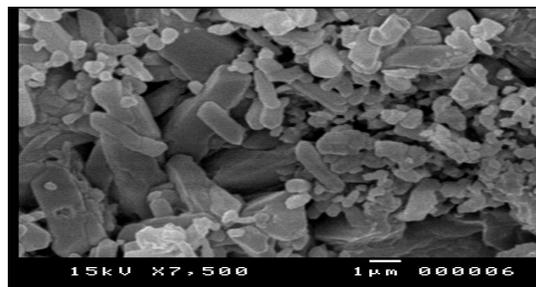


Fig. 20: Powder X-ray diffractograms of (A) pure drug KT, (B) HP- β -CD polymer, (C) physical mixture of KT with HP- β -CD 1:7, and (D) solid dispersion of KT with HP- β -CD 1:7.

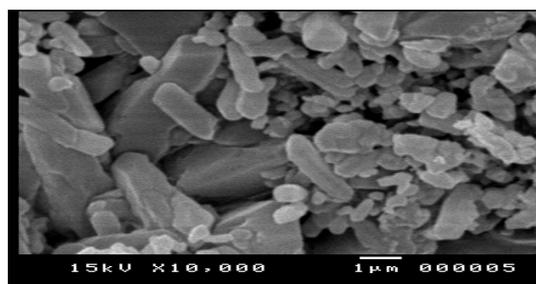
Scanning electron microscopy (SEM)

Photomicrographs of KT and KF/HP- β -CD solid dispersion 1:7 are shown in figure 21. The drug alone appeared as crystals of

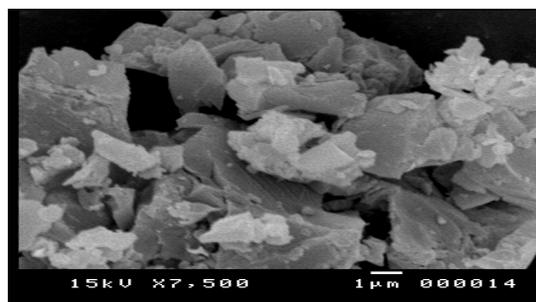
hexagonal shape. While KF/HP- β -CD solid dispersion revealed absence of crystalline structure of the drug. Thereby supporting the transformation of the drug into an amorphous state.



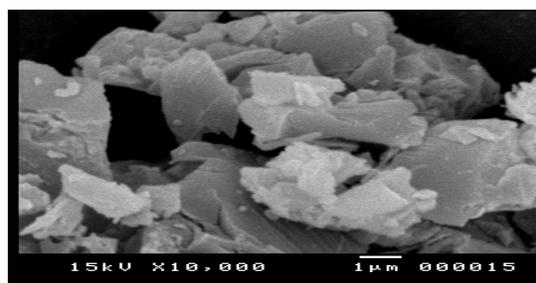
(A)



(B)



(C)



(D)

Fig. 21: SEM photomicrographs: (A) and (B) shows: pure drug KT; (C) and (D) shows: SD. of KT with HP- β -CD 1:7.

Conclusion

Ketotifen solid dispersions were prepared using Hydroxypropyl-Beta-Cyclodextrin (HP- β -CD), Pluronic 127 (PF-127), Pluronic 68 (PF-68), Polyethylene glycol 6000 (PEG 6000) and Polyethylene glycol 4000 (PEG 4000) at different ratios of drug: carrier (1:1, 1:3, 1:5 and 1:7) by solvent evaporation technique. The XRD and DSC studies indicated the transformation of crystalline KT (in pure drug) to amorphous KT by the solid dispersion technology. The saturation solubility and *in-vitro* dissolution studies showed a remarkable improvement in both the solubility as well as drug dissolution of these new KT solid dispersions than those of pure KT and KT physical mixtures. The best results obtained by the solid dispersion of KT with HP- β -CD in the ratio of drug: carrier 1:7. This study concluded that the improved solubility as well as drug dissolution of these newly prepared KT solid dispersions may be attributed to the decreased drug crystallinity, which can be modulated by appropriate level of hydrophilic carriers.

REFERENCES

- 1- C. Lipinski, "Poor aqueous solubility-an industry wide problem in drug delivery", *Am. Pharm. Rev.*, 5, 82-85 (2002).
- 2- C. Leuner and J. Dressman, "Improving drug solubility for oral delivery using solid dispersions", *Eur. J. Pharm. Biopharm.*, 50, 47- 60 (2000).
- 3- T. Ioftssona and D. Duchene, "Cyclodextrins in ophthalmic drug delivery", *Adv. Drug Deliv. Rev.*, 36 (1), 59-79 (1999).
- 4- Y. Aktas, N. Unlu, M. orphan, M. Irek and A. A. Hinkal, "Influence of hydroxyl propyl beta-cyclodextrin on the corneal permeation of pilocarpine", *Drug Dev. Ind. Pharm.*, 29, 223-230 (2003).
- 5- G. L. Amidon, H. Lennernas, V. P. Shah and J. R. Crison, "A theoretical basis for a biopharmaceutic drug classification: The correlation of *in-vitro* drug product dissolution and *in-vivo* bioavailability", *Pharm. Res.*, 12, 413-420 (1995).
- 6- M. K. Gupta, A. Vanwert and R. H. Bogner, "Formation of physically stable amorphous drugs by milling", *J. Pharm. Sci.*, 92, 536-551 (2003).
- 7- M. Otsuka and N. Kaneniwa, "Effect of grinding on the physicochemical properties of cephalexin", *Chem. Pharm. Bull.*, 32, 1079 (1984).
- 8- C. Cavallari, B. Abertini, M. L. Gonzalez-Rodriguez and L. Rodriguez, "Improved dissolution behaviour of steam granulated piroxicam", *Eur. J. Pharm. Biopharm.*, 54, 65-73 (2002).
- 9- J. R. Moyano, J. M. Gines, M. J. Arias and A. M. Rabasco, "Study of dissolution characteristics of oxazepam via complexation with β -cyclodextrin", *Int. J. Pharm.*, 114, 95-102 (1995).
- 10- O. I. Corrigan, "Thermal analysis of spray dried products", *Thermochim. Acta.*, 248, 245-258 (1995).
- 11- M. EL-Badry, M. Fathy and M. G. Abdel Mohsen, "Solubilization of some Non-Steroidal Anti inflammatory drugs (NSAIDs) by Pluronic F-127 block copolymer", *Bull. Pharm. Sci., Assiut University*, 27 (1), 1-9 (2004).
- 12- M. EI-Badry, M. A. Hassan, M. A. Ibrahim and H. Elsaghir, "Performance of Poloxamer 407 as Hydrophilic Carrier on the Binary Mixtures with Nimesulide", *FARMACIA*, 61 (6), 1137-1150 (2013).
- 13- E. A. Fouad, M. EL-Badry, G. M. Mahrous, F. K. Alanazi, S. H. Neau and I. A. Alsarra, "The use of spray-drying to enhance celecoxib solubility", *Drug Development and Industrial Pharmacy*, 37 (12), 1463-1472 (2011).
- 14- A. A. Ambike, K. K. Mahadik and A. Paradkar, "Stability study of amorphous valdecoxib", *Int. J. Pharm.*, 282, 151-162 (2004).
- 15- A. Paradkar, A. A. Ambike, B. K. Jadhav and K. K. Mahadik, "Characterization of curcumin-PVP solid dispersion obtained by spray drying", *ibid.*, 271, 281-286 (2004).
- 16- C. Leuner and J. Dressman, "Improving drug solubility for oral delivery using solid dispersions", *Eur. J. Pharm. Biopharm.*, 50, 47- 60 (2000).
- 17- D. Q. M. Craig, "The mechanisms of drug release from solid dispersions in water soluble polymers", *Int. J. Pharm.*, 231, 131-144 (2002).
- 18- A. V. Kapanov, E. V. Batrakova and V. Y. Alakhov, "Pluronic block copolymers as

- novel polymer therapeutics for drug and gene delivery", *J. Control. Rel.*, 82, 189-212 (2002).
- 19- W. L. Chiou and S. Rielman, "Pharmaceutical application of solid dispersion system", *J. Pharm. Sci.*, 60, 1281-1302 (1971).
 - 20- F. Damian, N. Blaton, L. Naesens, *et al.*, "Physicochemical characterization of dispersions of the antiviral agent UC-781 with Polyethylene glycol 6000 and Gelucire 44/14", *Eur. J. Pharm. Sci.*, 10, 311-322 (2000).
 - 21- J. L. Ford, "The Current states of Solid dispersions", *Pharm. Acta. Helv.*, 61, 69-88 (1986).
 - 22- N. Zerrouk, C. Chemtob, P. Arnaud, S. Toscani and J. Dugue, "*In-vitro* and *in-vivo* evaluation of carbamazepine-PEG 6000 solid dispersions", *Int. J. Pharm.*, 225, 49-62 (2001).
 - 23- B. M. Tashtoush, Z. S. Al-Quashi and N. M. NaWib, "*In-vitro* and *in-vivo* evaluation of glibenclamide in solid dispersion systems", *Drug Dev. Ind. Pharm.*, 30, 601-607 (2004).
 - 24- G. Van den Mooter, "Evaluation of Inutec SPI as new carrier in the formulation of solid dispersion of poorly soluble drugs", *Int. J. Pharm.*, 316, 1-6 (2006).
 - 25- A. Das, A. K. Nayak, B. Mohanty and S. B. Panda, "Solubility and dissolution enhancement of etoricoxib by solid dispersion technique using sugar carriers", *ISRN Pharmaceutics*, Art. No. 819765 (2011).
 - 26- L. P. Craps and U. M. Ney, "Ketotifen: Current views on its mechanism of action and their therapeutic implications", *Respiration*, 45 (4), 411-421 (1984).
 - 27- M. A. Sayeed, F. M. Farhad, S. M. Tareq, M. Ikram, M. N. Islam, S. A. Siddique and D. Das, "A study of *in-vitro* interaction of ketotifen fumarate with Domperidone at different gastric and intestinal PH", *Russian Open Medical Journal*, 3 (0204), 1-6 (2014).
 - 28- K. Inoue, K. Ogawa, Y. Suzuki, J. Okada, A. Kusai, M. Ikeda and K. Nishimura, "The skin permeation mechanism of ketotifen: Evaluation of permeation pathways and barrier components in the stratum corneum", *Drug Dev. Ind. Pharm.*, 26 (1), 45-53 (2000).
 - 29- A. Grahnen, A. Lonnebo, O. Beck, S. A. Eckernas, B. Dahlstrom and B. Lindstrom, "Pharmacokinetics of ketotifen after oral administration to healthy male subjects", *Biopharm. Drug Dispos.*, 13 (4), 255-262 (1992).
 - 30- S. A. EL-Harras, "*In-vitro* release of freeze-dried mefenamic acid poloxamer from suppository bases and evaluation of its anti inflammatory effect", *Bull. Pharm. Sci., Assuit University*, 20 (1), 95-104 (1997).
 - 31- Z. Mihun, J. Kuftinec, H. Hofman, M. Zinic and F. Kajfez, "Ketotifen", In: "Analytical Profile of Drug Substances", K. Florey (Ed.), Academic Press, Inc., London, UK, Vol. 13, 1984, pp. 240-262.
 - 32- S. W. Jun, M. S. Kim, J. S. Kim, H. J. Park, S. Lee, J. S. Woo and S. J. Hwang, "Preparation and characterization of simvastatin/hydro-xypropyl- β -cyclodextrin inclusion complex using supercritical antisolvent (SAS) process", *Eur. J. Pharm. Biopharm.*, 66 (3), 413-421 (2007).
 - 33- M. Fathy and M. Elbadry, "Preparation and Evaluation of Piroxicam- pluronic solid dispersion", *Bull. Pharm. Sci., Assuit University*, 26 (2), 97-108 (2003).
 - 34- M. Elbadry, G. Fetih and M. Fathy, "Improvement of solubility and dissolution rate of Indomethacin by solid dispersions in Gelucire 50/13 and PEG 4000", *Saudi Pharmaceutical Journal*, 17, 217-225 (2009).
 - 35- M. A. Bayomi, K. A. Abanumay and A. A. Al- Angary, "Effect of inclusion complexation with cyclodextrins on photostability of nifedipine in solid state", *Int. J. Pharm.*, 243 (1-2), 107-117 (2002).
 - 36- L. Wang, L. C. Rui and J. X. Hua, "*In situ* intestinal absorption behaviors of Tanshinone IIA from its inclusion complex with hydroxyl propyl- β -cyclodextrin", *Biol. Pharm. Bull.*, 30 (10) 1918-1922 (2007).



نشرة العلوم الصيدلانية جامعة أسيوط



تحسين ذوبانية عقار الكيتوتيفين في الماء وزيادة معدل إتاحتة في المحلول

فرجاني عبد الحميد محمد محمد - دينا فتح الله محمد - أمنية علي السيد

قسم الصيدلانيات ، كلية الصيدلة ، جامعة أسيوط ، أسيوط ، مصر

تم إجراء دراسة مقارنة لتحضير ودراسة خصائص المشتتات الصلبة والحبيبات المذبية وقياس معدل إتاحة العقار في المحلول من هذه النظم. في هذه الدراسة تم استخدام بوليمر الهيدروكسي بروبائل بيتا سيكلودكسترين وعديدات الايثيلين جليكول ذات الاوزان الجزيئية (٤٠٠٠، ٦٠٠٠) وكذلك البلورنك (ف ٦٨، ف ١٢٧) بنسب وزنية مختلفة ولتحقيق ذلك الهدف اشتملت الدراسة على:

- ١- تحضير المشتتات الصلبة والحبيبات المذبية من العقار مع الهيدروكسي بروبائل بيتا سيكلودكسترين وعديدات الايثيلين جليكول والبلورنك بنسب وزنية (١:١، ١:٣، ١:٥، ١:٧) (حامل:عقار).
- ٢- توصيف هذه النظم المحضرة ودراسة خواصها الفيزيوكيميائية وذلك لتوضيح طبيعة التفاعل بين العقار والبوليمرات التي تذوب في الماء. وقد تم ذلك باستخدام عدة طرق منها القياس بالاشعة تحت الحمراء ، التحليل الحراري ، حيود الاشعة السينية ، والتصوير باستخدام الميكروسكوب الالكتروني. وكانت النتائج كالتالي:
- دلت طريقة القياس بالاشعة تحت الحمراء على توافق العقار مع الجزيئات الكبيرة محل الدراسة.
- أوضحت طريقتنا التحليل الحراري وحيود الأشعة السينية أن لهما نفس السلوك الحراري مثل مخلوطهما الفيزيائي الذي له نفس النسب الوزنية وقد أوضحت أيضاً هذه الدراسة ان العقار قد ذاب في البوليمرات المنصهرة.
- أوضحت طرق حيود الأشعة السينية والتحليل الحراري والميكروسكوب الالكتروني نقص درجة التبلور للعقار نتيجة لتكون المشتتات الصلبة والحبيبات المذبية للعقار مع البوليمرات التي تذوب في الماء.
- ٣- خصائص معدل إتاحة العقار من النظم المحضرة مع البوليمرات التي تذوب في الماء: تم قياس معدل إتاحة الكيتوتيفين من النظم موضوع الدراسة ومقارنته بمخلوطه الفيزيائي مع البوليمرات طبقاً لطريقة الكمية المنتشرة في محلول الفوسفات المنظم ذي الأس الهيدروجيني (٤، ٧) ، وقد أوضحت نتائج الدراسة التالي:
- معدل إتاحة العقار من النظم المحضرة مع بوليمر الهيدروكسي بروبائل بيتا سيكلودكسترين وعديدات الايثيلين جليكول والبلورنك كان أعلى بصورة ملحوظة من معدل إتاحة العقار بمفرده.
- وجد انه كلما زادت نسبة المادة الحاملة في النظم المحضرة زاد معدل إتاحة العقار.
- تم الوصول لأعلى معدل إتاحة للعقار من النظم المحضرة مع بوليمر الهيدروكسي بيتا سيكلودكسترين بنسبة وزنية (١:٧) (حامل:عقار).